

Dissipative Particle Dynamics

Some Recent Developments

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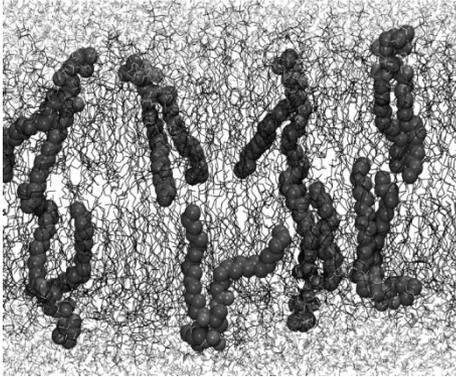
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November 30, 2016

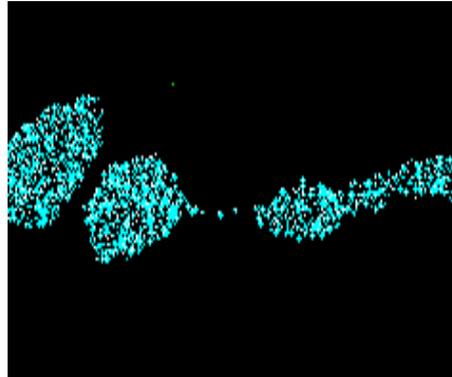
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- 1. Background**
- 2. Recent developments in methodology**
- 3. Micro drop dynamics with DPD**
- 4. Multiphase flows with DPD**
- 5. Complex fluids in micro channels**
- 6. Modeling single cells with DPD**
- 7. Conclusions**

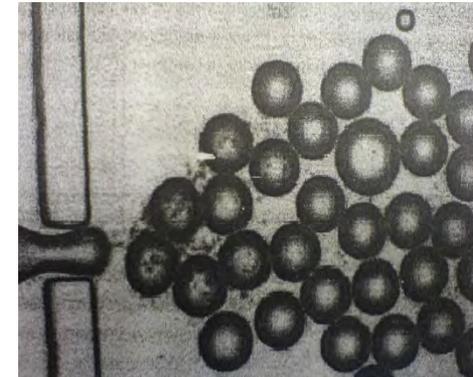
1.1 Meso & multiple scale problems



Cross section of a bilayer of lipid in water molecules



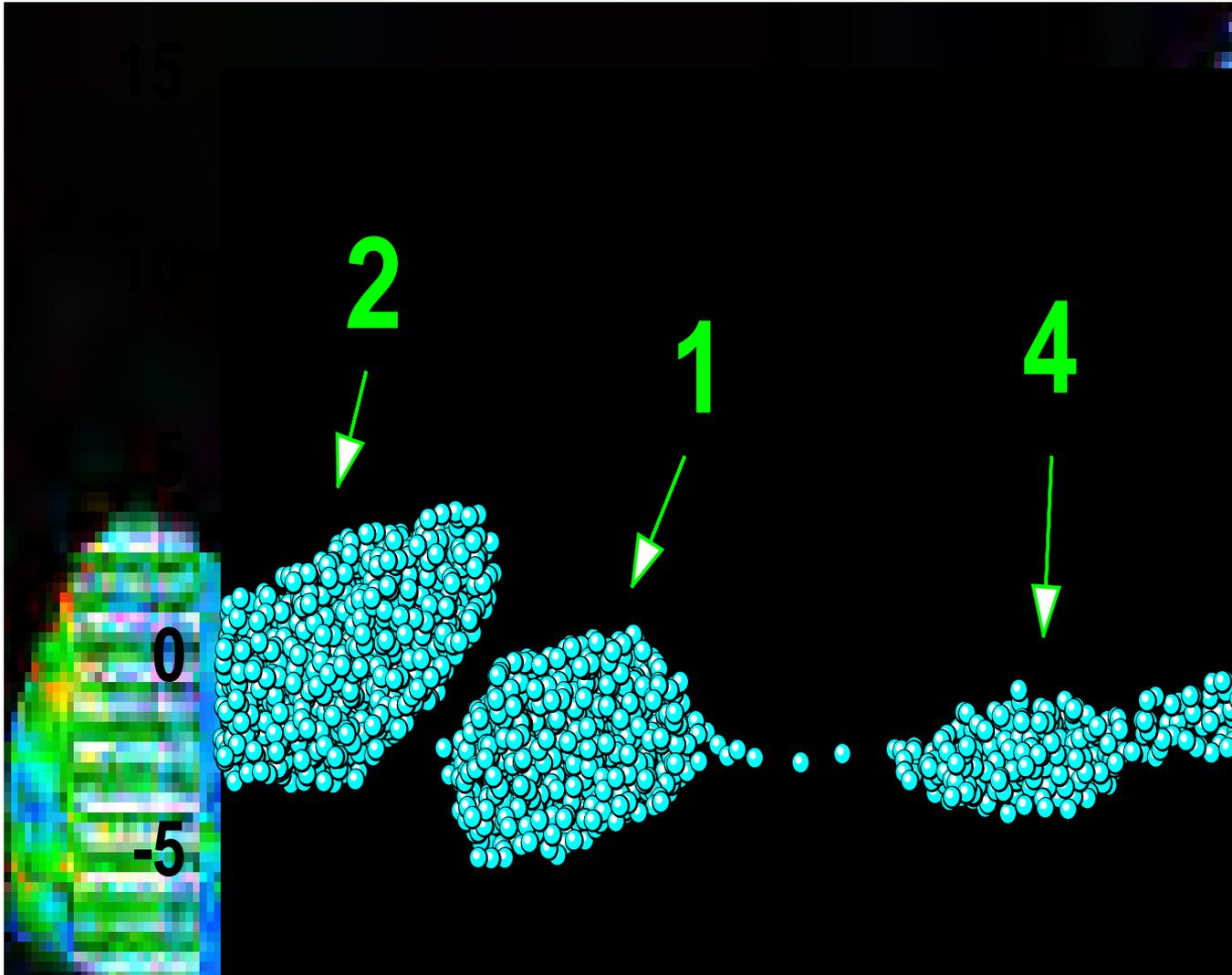
Evolution of a polymer drop break-up



Water droplets in oil

- ❑ Numerical methods based on continuum scale constitutive equations may not be valid when the dimension diminishes,
- ❑ Conventional MD is heavily restricted from practical applications due to the extremely small time scales (**nanoseconds**) and length scales (**nanometers**).
- ❑ How to increase computational ability:
 - 1、 High performance computing with thousands of processors,
 - 2、 New computational methods which can be realizable for bigger scales.

1.2 Particle methods at different scales



1. Background

1.3 General features of particle methods

- Individual particles are used to represent a volume of fluid that may vary in size, depending on the model, from a single atom/molecule (in MD), a small cluster of atoms or molecules (in DPD), to a macroscopic region in a continuum solid or fluid (in SPH).
- Masses are centered on particles.
- Particles move with local velocity of the fluid — Lagrangian nature.
- Forces are usually calculated from particle interactions either using an interaction potential (DPD) or some kind of weight function (SPH) with a cutoff distance.

Particle-Particle Interaction

1. Background

1.4 SPH – Methodology

History

- Originally invented for solving astrophysical problems in open space
- Recently applied to general fluid dynamic problems

Numerical approximation

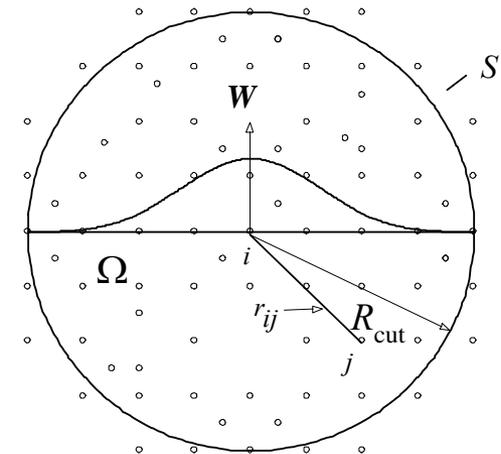
- Weight function (or smoothing function), W , centered on particles and describe continuous or discrete field function,

- **Kernel approximation:**

$$f_i \cong \int f(\mathbf{x})W_i(\mathbf{x})d\mathbf{x} \quad f_{i,\alpha} \cong \int f(\mathbf{x})W_{i,\alpha}d\mathbf{x}$$

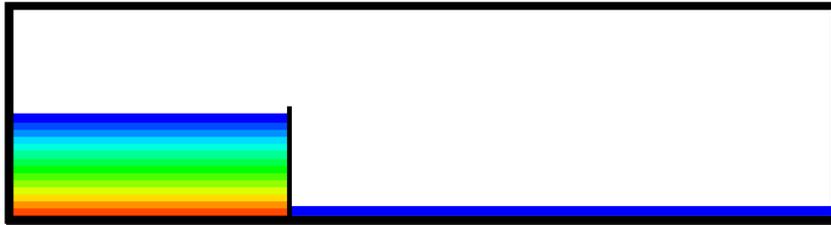
- **Particle approximation:**

$$f_i \cong \sum_{j=1}^N f_j W_{ij} m_j / \rho_j \quad f_{i,\alpha} \cong \sum_{j=1}^N f_j W_{i,\alpha} m_j / \rho_j$$

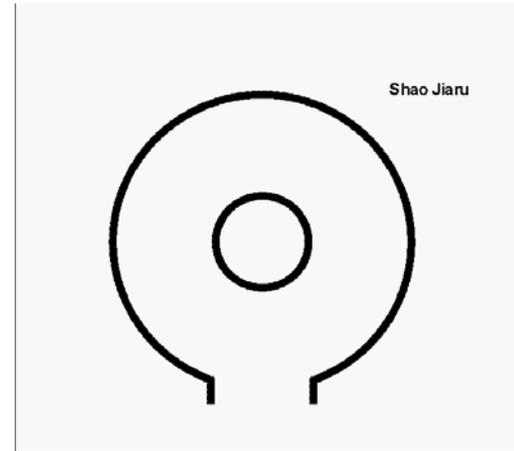


SPH approximations in a two-dimensional space

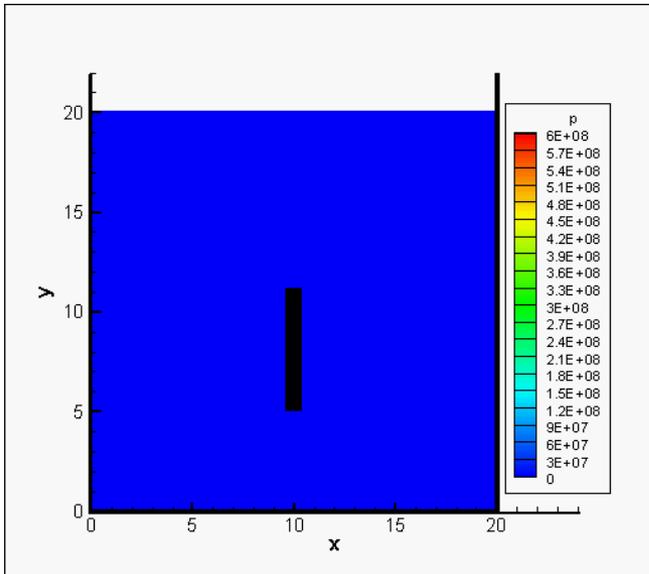
1.4 SPH – Applications



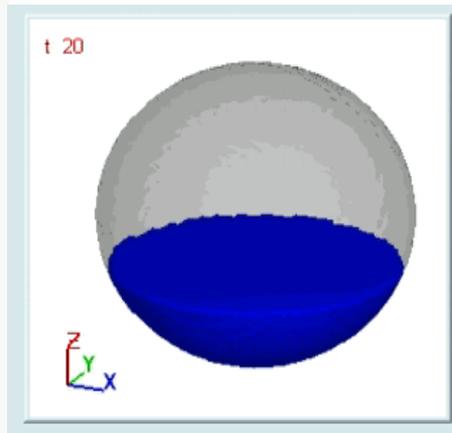
Water discharge



Injection flow



Water exit

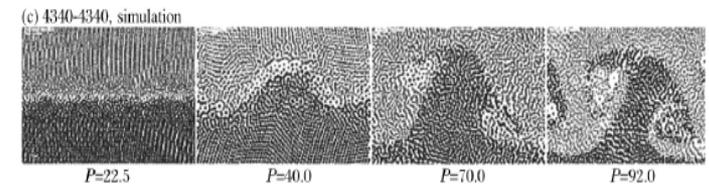
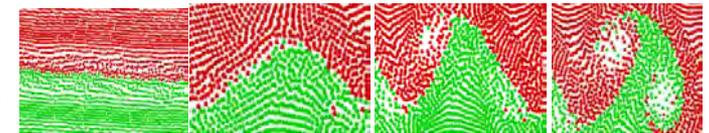
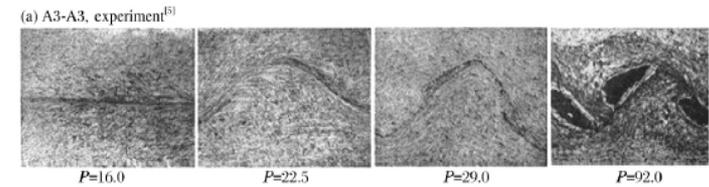
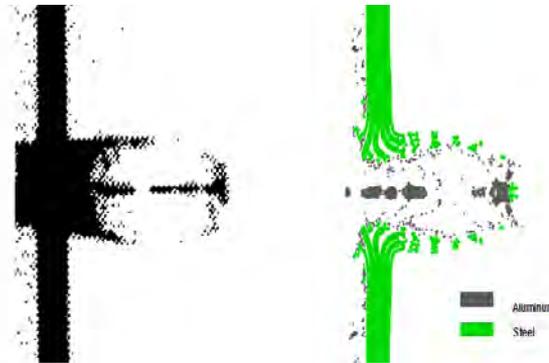
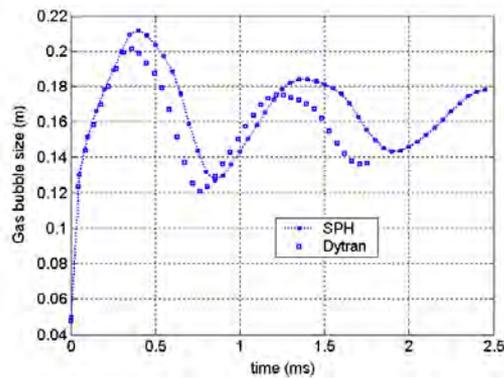
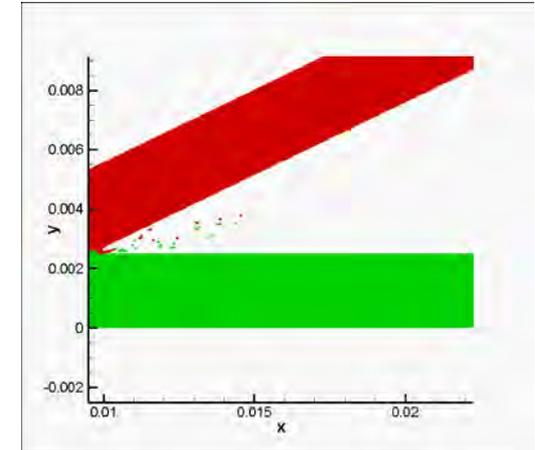
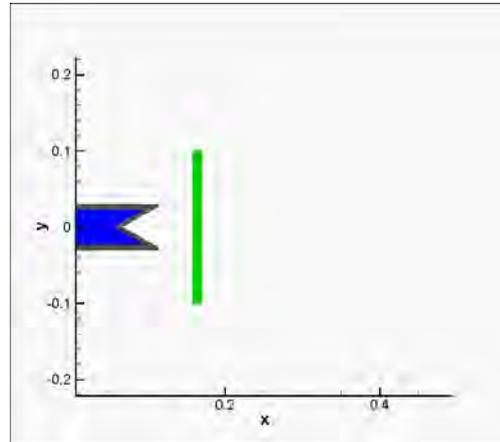
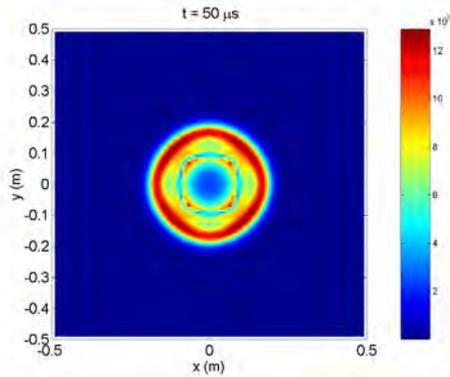


Liquid sloshing



Oil spill and boom movement

1.4 SPH – Applications



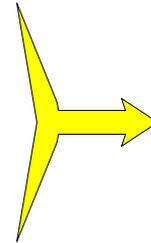
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Shaped charge jet

Explosive welding

1.5 DPD-dissipative particle dynamics

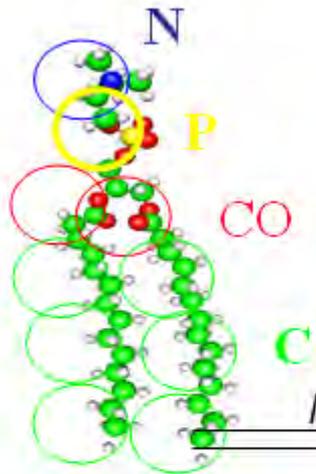
- a. Coarse-grained MD
- b. A cluster of atoms/molecules
- c. Soft interactions
- d. Applications:
 - colloidal suspension
 - Surfactant
 - dilute polymer solutions
 - biological membranes
 - macromolecular movements



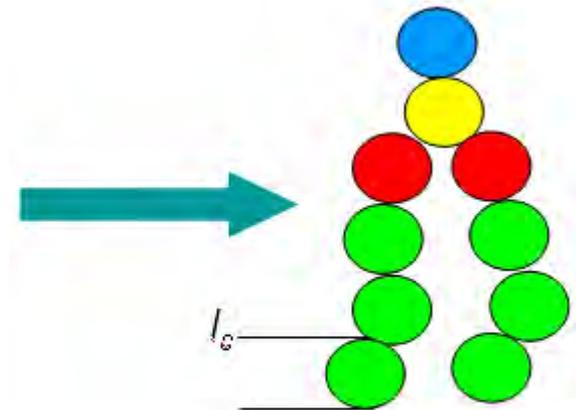
More efficient
than MD (larger
time step & scale)

A model of lipid
Maximum time-step

$$\Delta t_{\max} \sim l \sqrt{\frac{m}{k_B T}}$$



All-atom model
118 atoms



Coarse-grained model
10 sites

2.1 Governing equations

$$\frac{d\mathbf{r}_i}{dt} = \mathbf{v}_i, \quad \frac{d\mathbf{v}_i}{dt} = \mathbf{f}_i = \mathbf{f}_i^{int} + \mathbf{f}_i^{ext} \quad \mathbf{f}_i^{int} = \sum_{j \neq i} \mathbf{F}_{ij} = \sum_{j \neq i} \mathbf{F}_{ij}^C + \mathbf{F}_{ij}^D + \mathbf{F}_{ij}^R$$

Conservative force

$$\mathbf{F}_{ij}^C = a_{ij} w^C(r) \hat{\mathbf{r}}_{ij}$$

Dissipative force

$$\mathbf{F}_{ij}^D = -\gamma w^D(r_{ij}) (\hat{\mathbf{r}}_{ij} \cdot \mathbf{v}_{ij}) \hat{\mathbf{r}}_{ij}$$

Random force

$$\mathbf{F}_{ij}^R = \sigma w^R(r_{ij}) \xi_{ij} \hat{\mathbf{r}}_{ij}$$

**Fluctuation-
Dissipation
theorem**

$$w^D(r) = [w^R(r)]^2, \quad \gamma = \frac{\sigma^2}{2k_B T},$$

2. DPD – Method development

2.2 Constructing new DPD interaction

1. **Conventional** conservative weight function $W_c(r) = 1 - r$

Corresponding potential $U(r) = 0.5 - (r - 0.5r^2)$

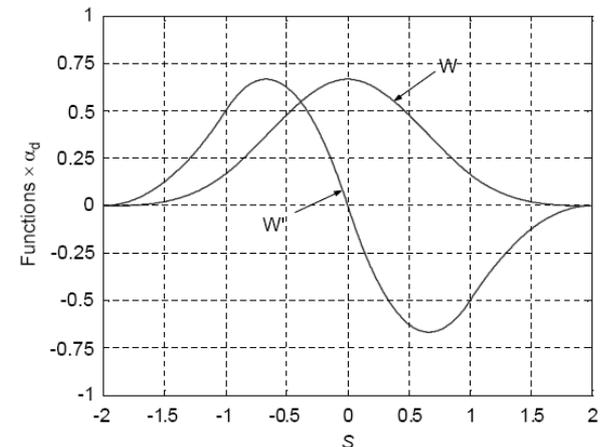


Purely repulsive, only for gas

2. **New** conservative interaction potential

$$U(r) = AW_1(r) - BW_2(r) = AW_1(r, r_{c1}) - BW_2(r, r_{c2})$$

W , SPH smoothing function

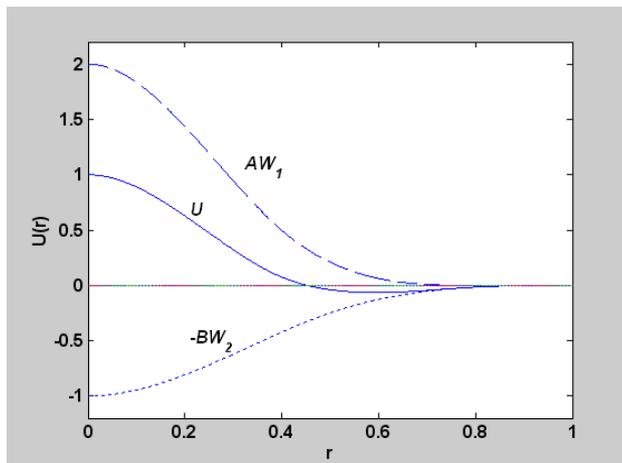


➤ $W(r)$: purely repulsive, $-W(r)$: purely attractive

➤ U shape $\leftarrow A, B, r_{c1}, r_{c2}$

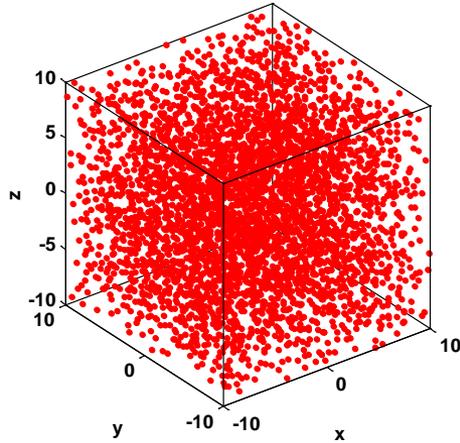
➤ Fluid properties \leftarrow U shape

➤ It is feasible to model liquid/gas co-existing systems like multiphase fluid transport.

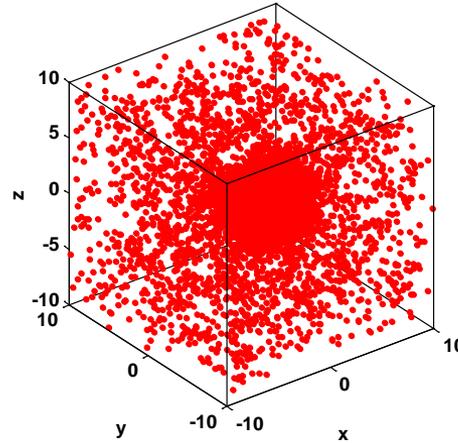


2. DPD – Method development

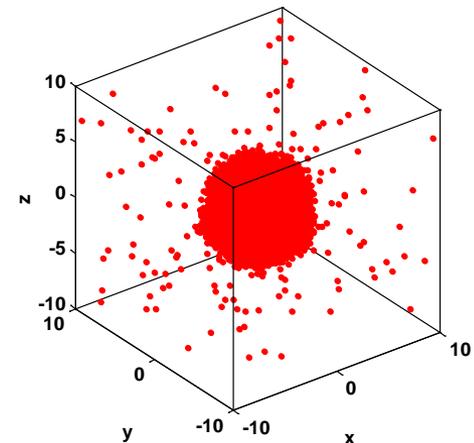
$$U(r) = 18.75[2W_1(r, 0.8) - BW_2(r, 1.0)] \rightarrow \text{Surface tension}$$



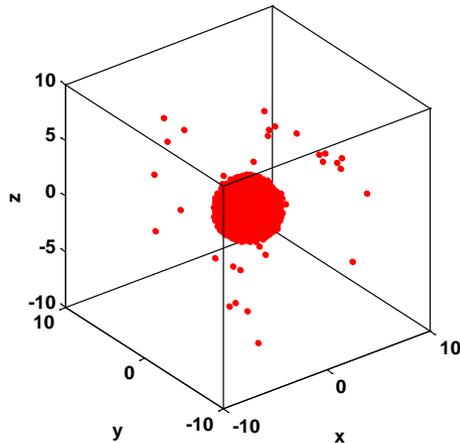
B = 0.0



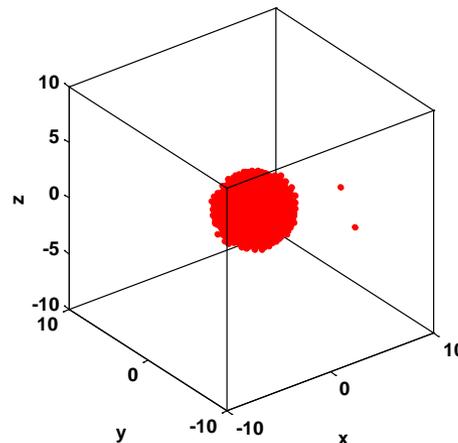
B = 0.5



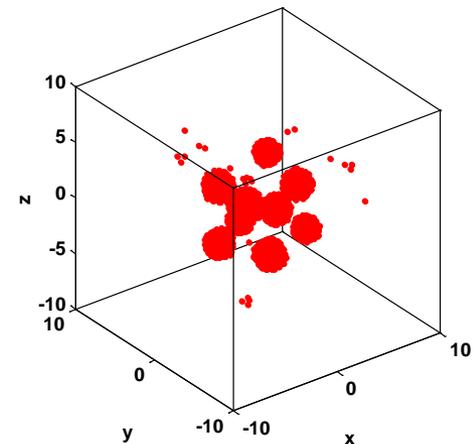
B = 0.9



B = 1.0



B = 1.05

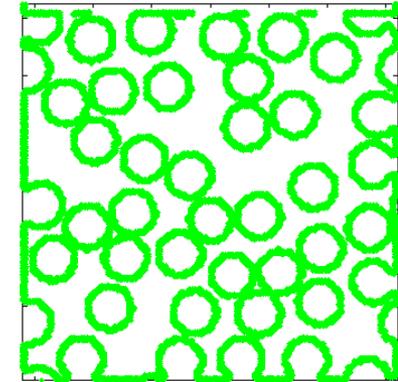
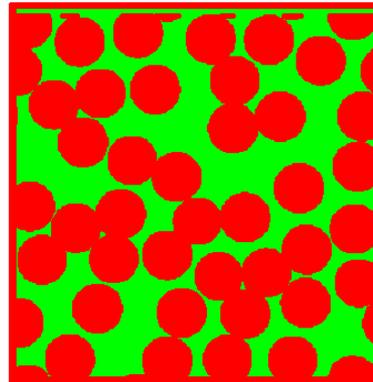


B = 1.20

Different interaction parameters determines different fluid properties.

2.3 Treating complex solid boundary

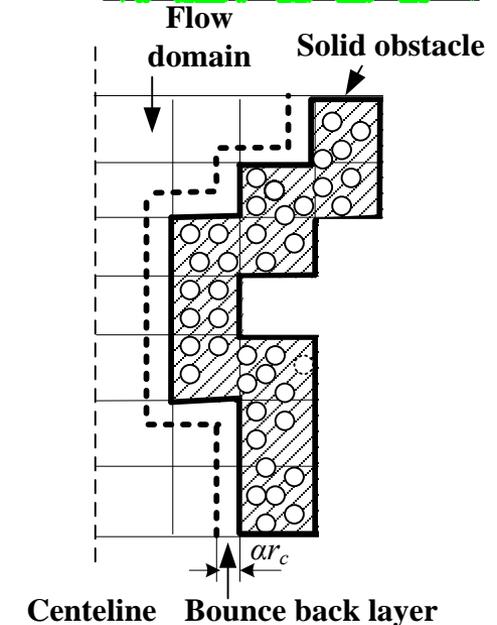
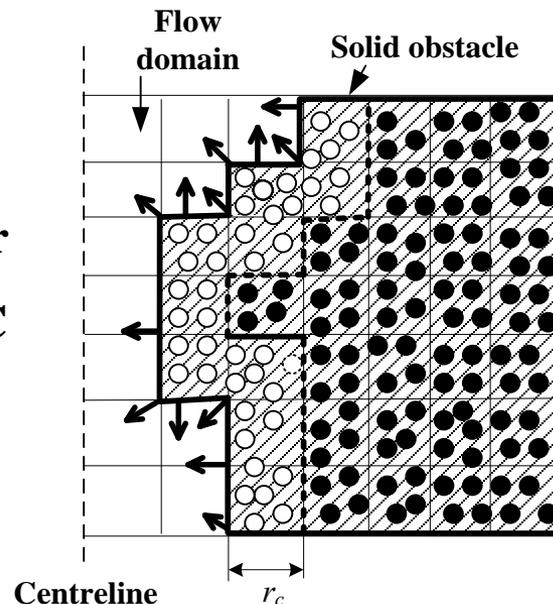
1. Solid matrix



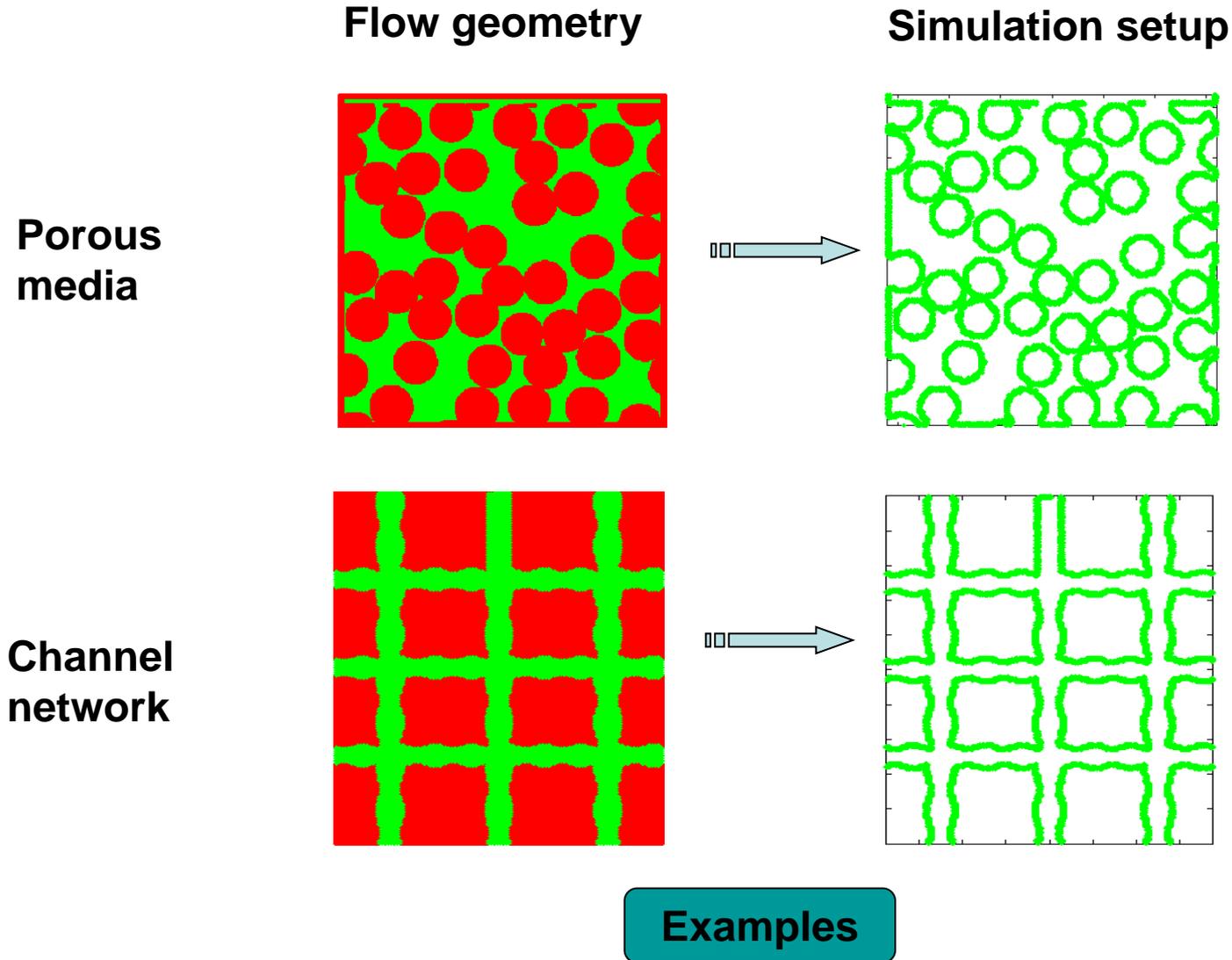
2. Solid boundary

a. fluid boundary layer

b. reflective/mirror BC



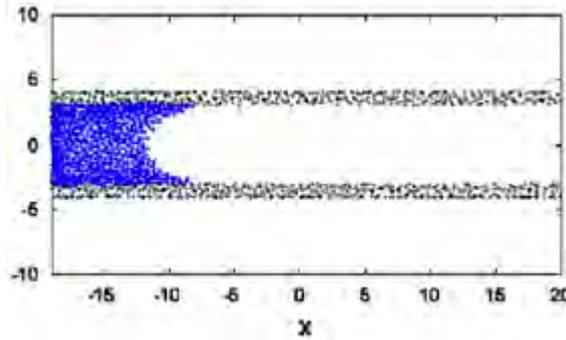
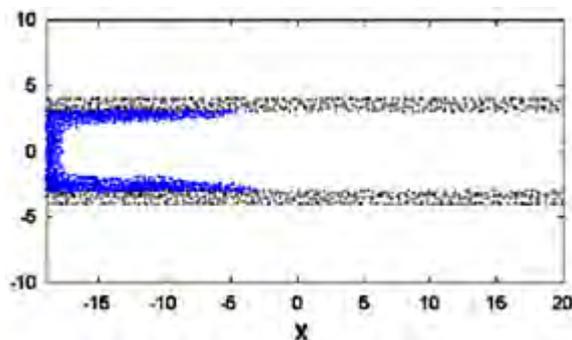
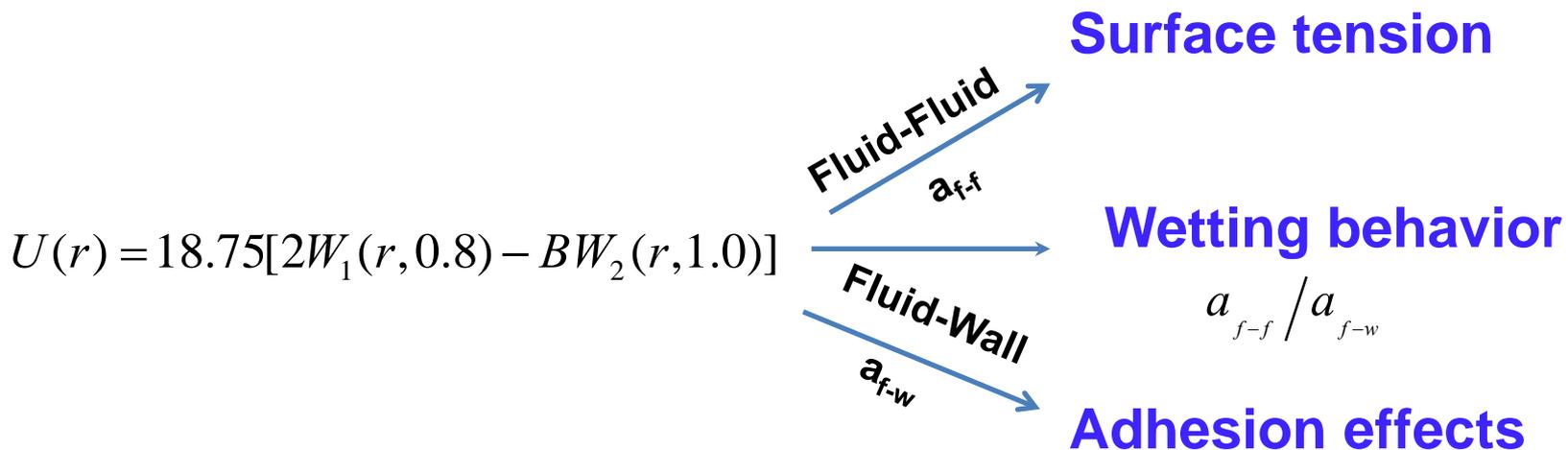
2. DPD – Method development



2. DPD – Method development

2.4 Modeling wetting phenomenon

The particle-particle interactions between fluid-solid and fluid-fluid determine the contact line dynamics and wetting behavior



Different strength ratio leads to different wetting behaviors

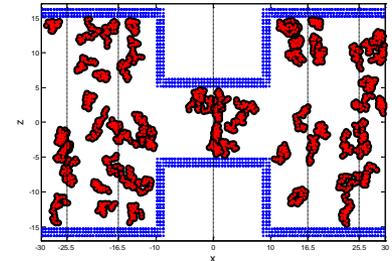
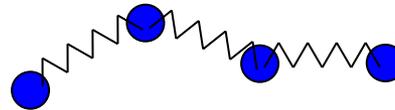
2.5 Modeling chained or net structure

Bead-Chain Model

When modeling complex fluids (macromolecules like DNA), it is possible to use bead-chain model to simulate the interaction between chained particles.

The FENE (finitely extendible nonlinear elastic) model

$$\mathbf{F}_{ij}^S = \frac{H\mathbf{r}_{ij}}{1 - (r_{ij}/r_{\max})^2}$$



Other models like [worm-like chain \(WLC\)](#)

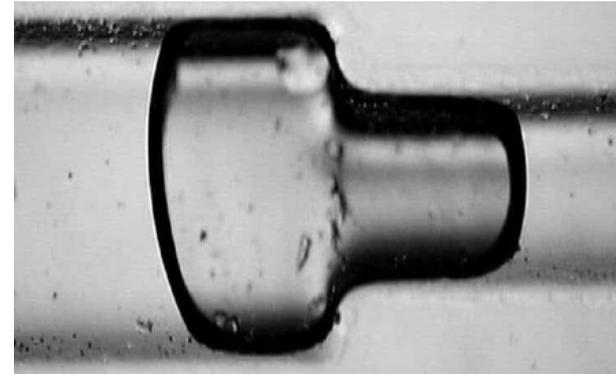
Can further consider length and angle, and surface energy...

3. Micro drop dynamics with DPD

- liquid drop and associated phenomena widely exist: ink-jet printing, enhanced oil recovery, soil erosion, and fuel injection atomization...



water droplet on lotus leaf



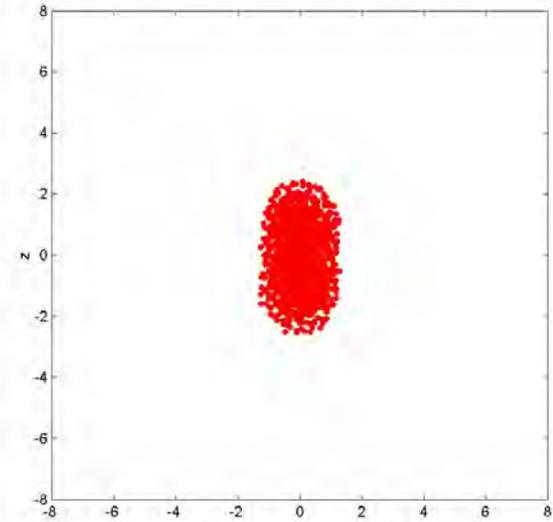
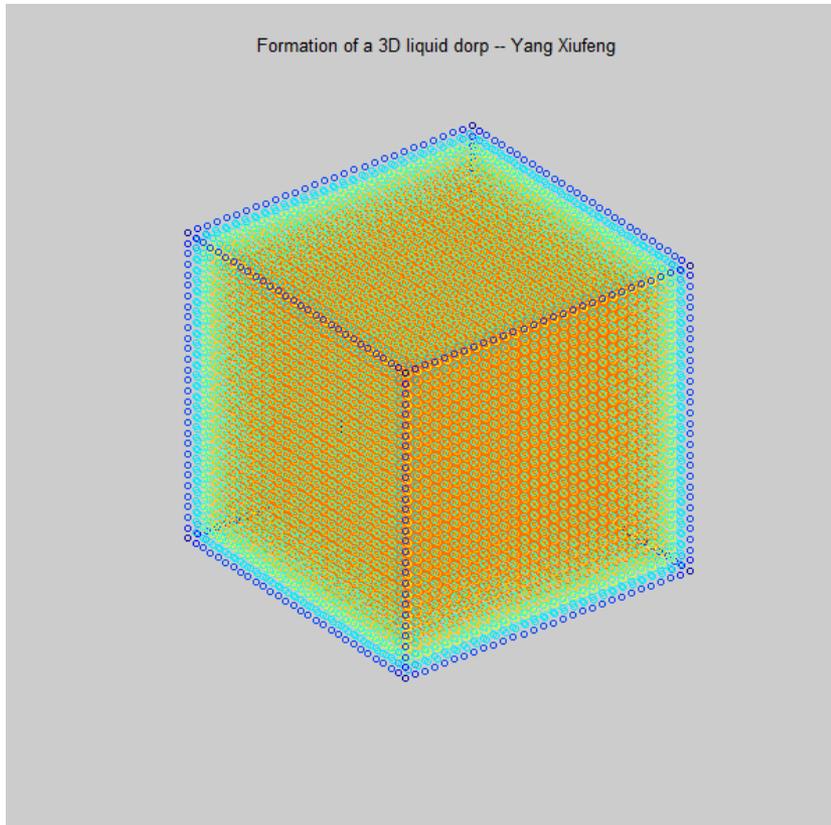
Liquid drop stuck in a micro channel due to non-wetting effects



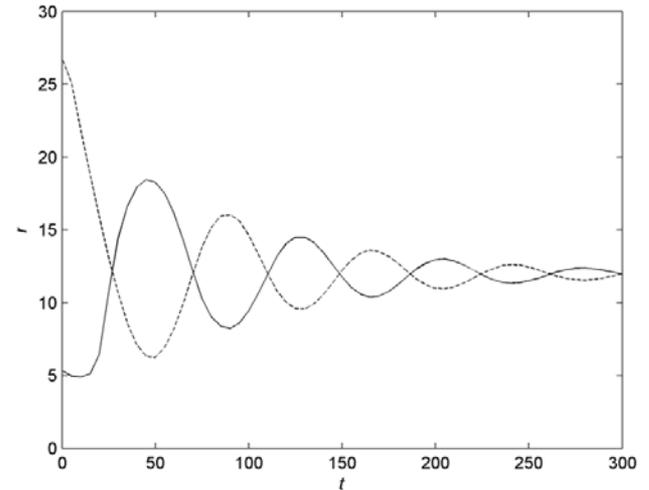
water droplet on a caterpillar

3. Micro drop dynamics with DPD

Formation of liquid drop



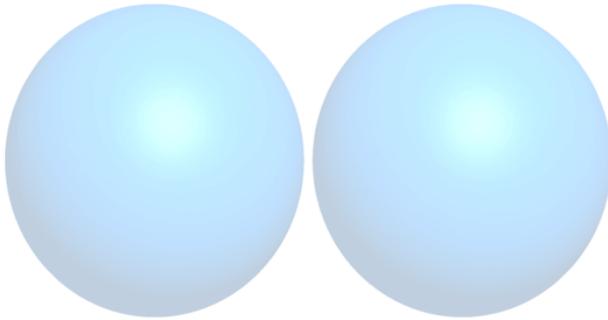
Liquid drop oscillation



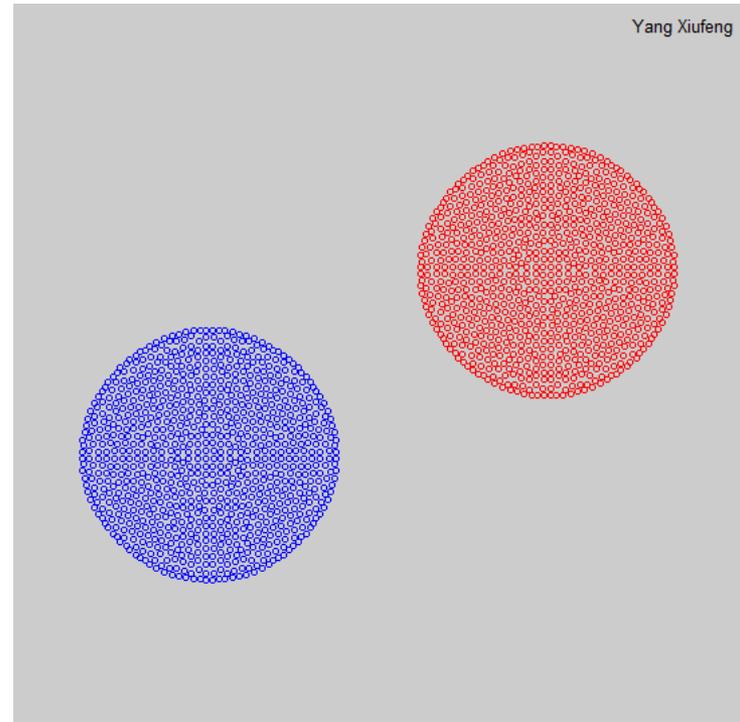
Evolution of axis

3. Micro drop dynamics with DPD

Head-on collision

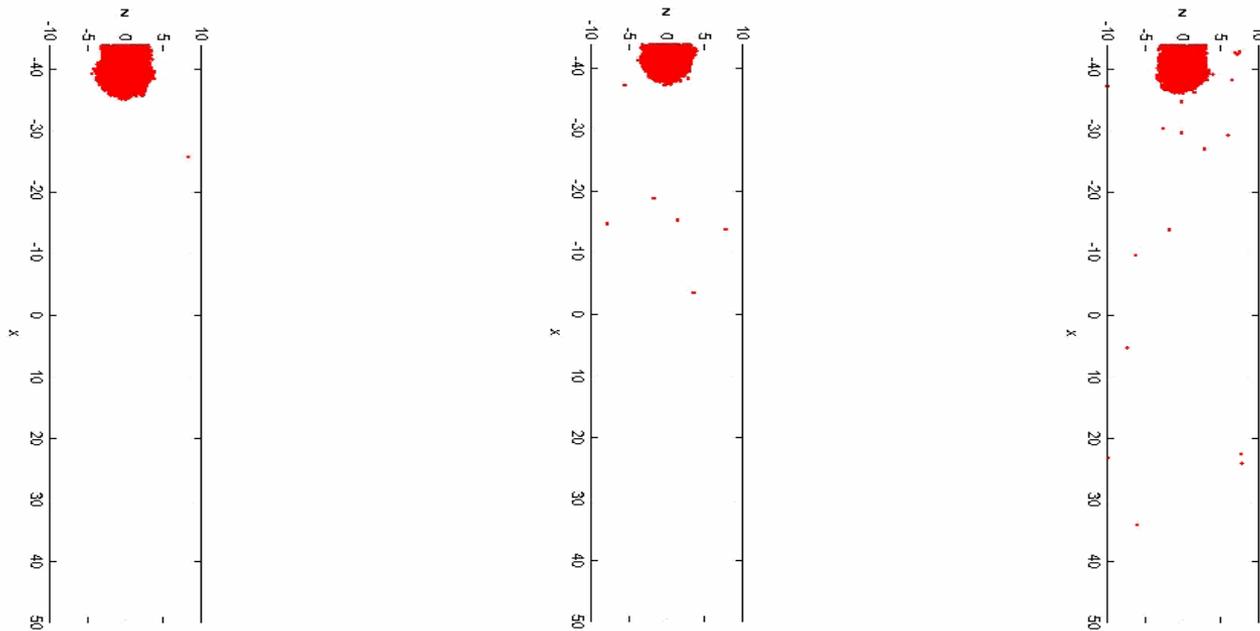


Off-center collision



3. Micro drop dynamics with DPD

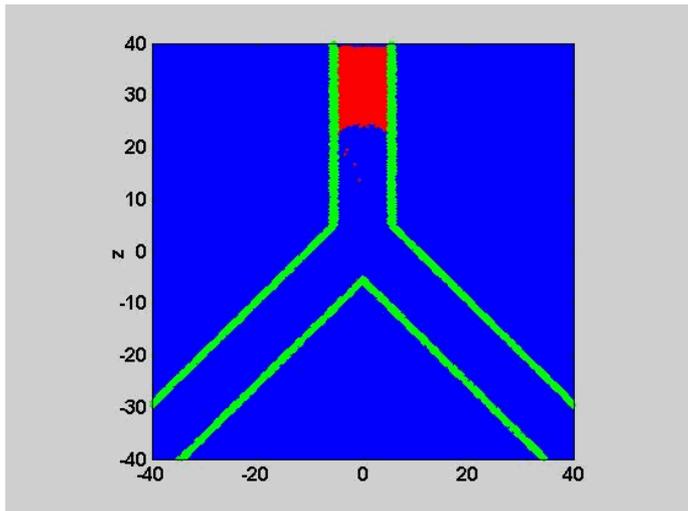
Dripping flow



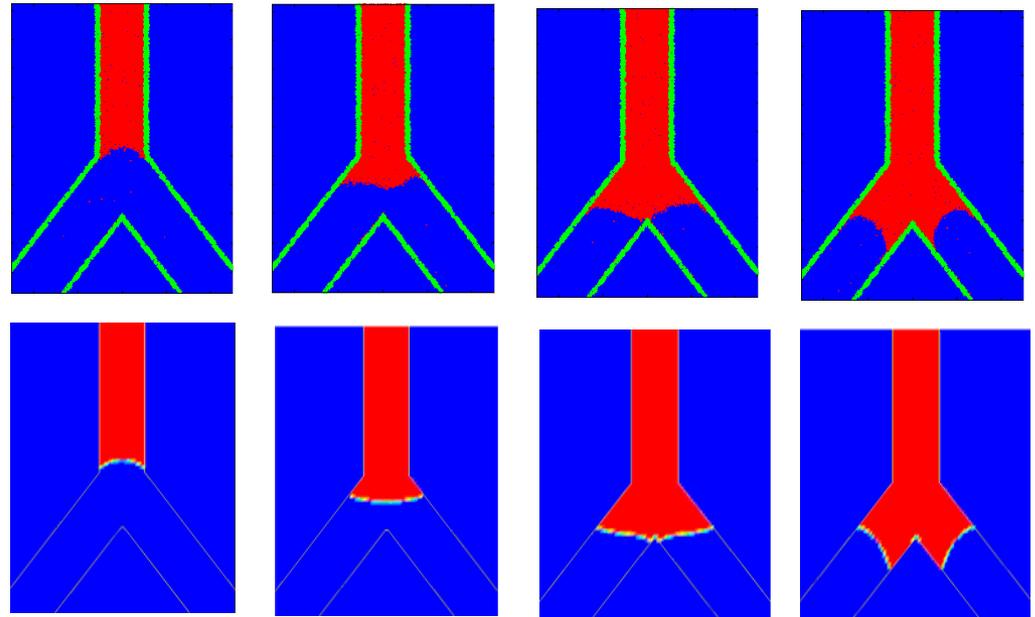
Continuous flow → dripping flow → liquid drops

4. Multiphase flows with DPD

4.1 Two phase flow – Inverted Y channel



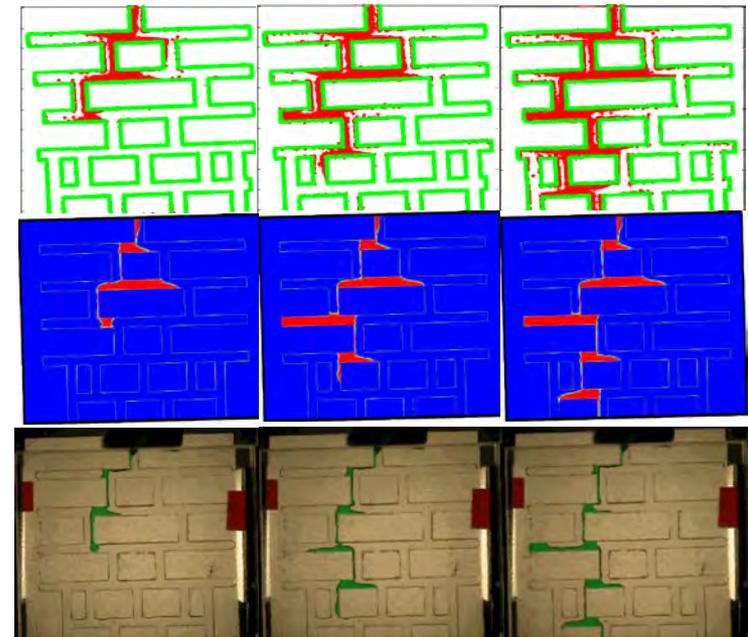
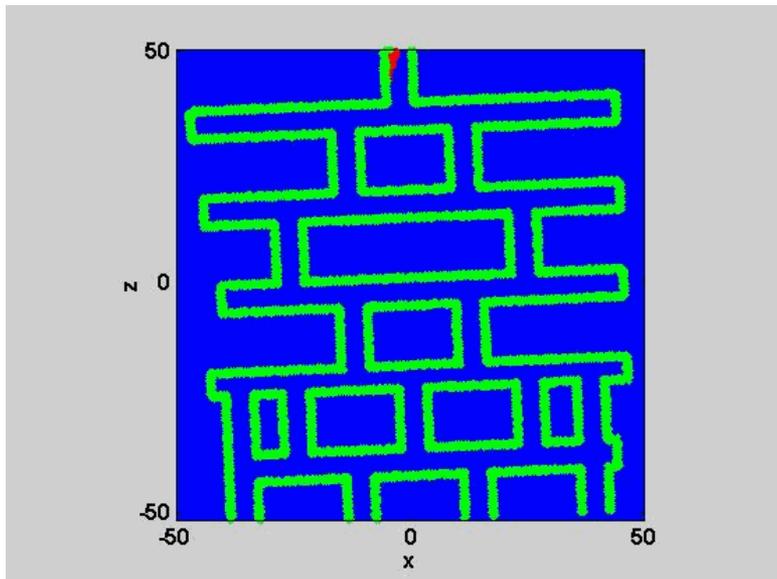
DPD VS VOF



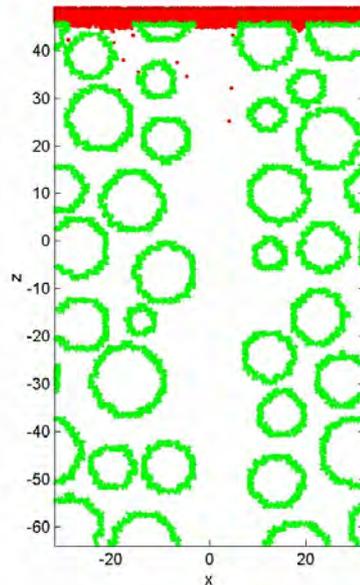
4. Multiphase flows with DPD

4.2 Two phase flow – channel network

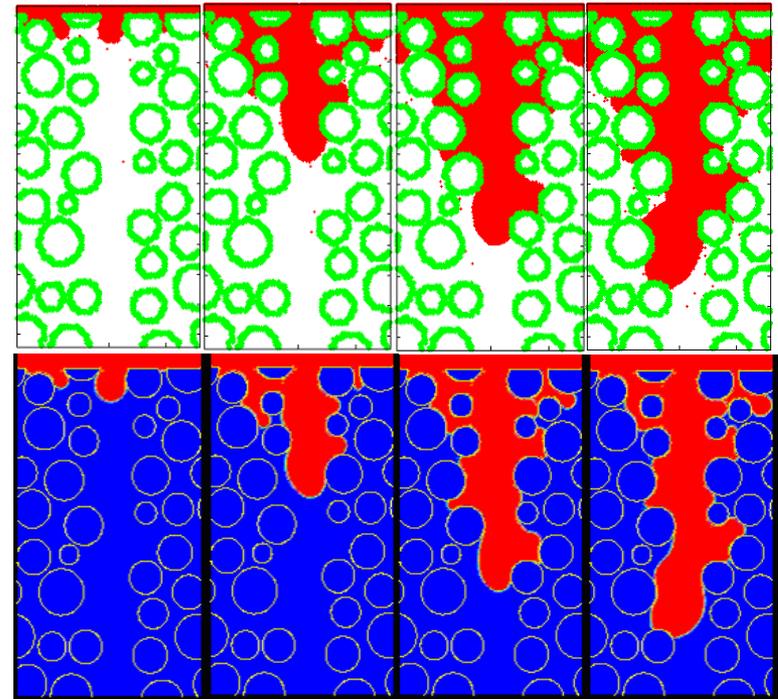
DPD VS VOF, Experiment



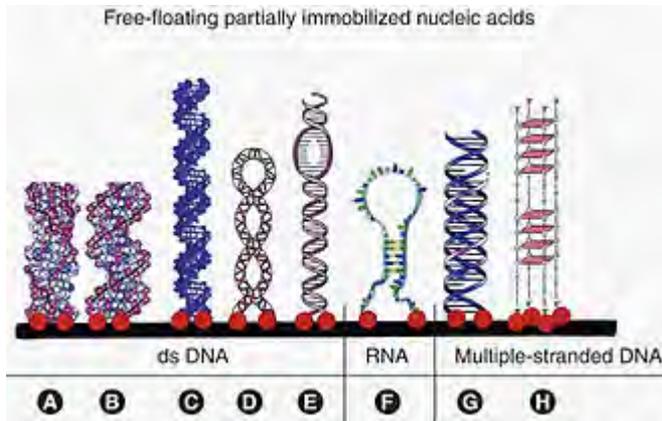
4.3 Two phase flow – Porous media



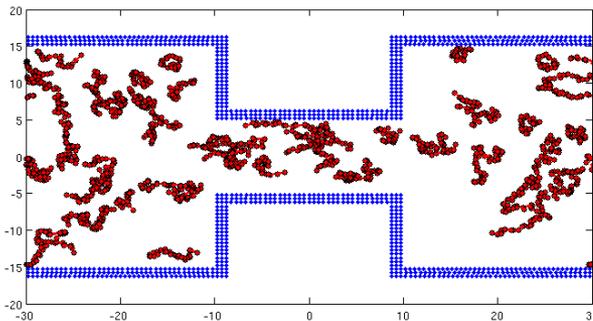
DPD VS VOF



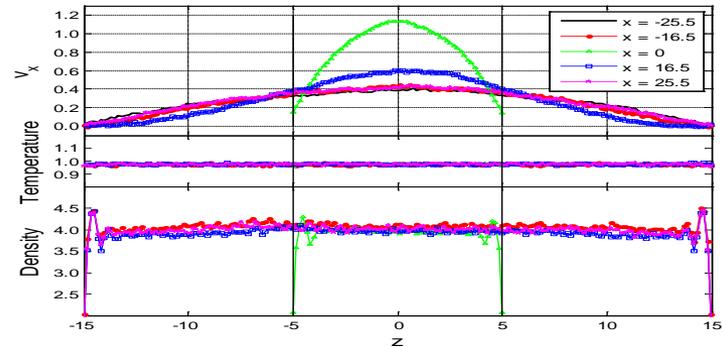
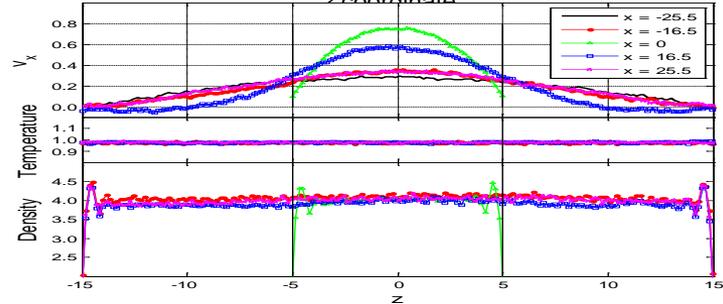
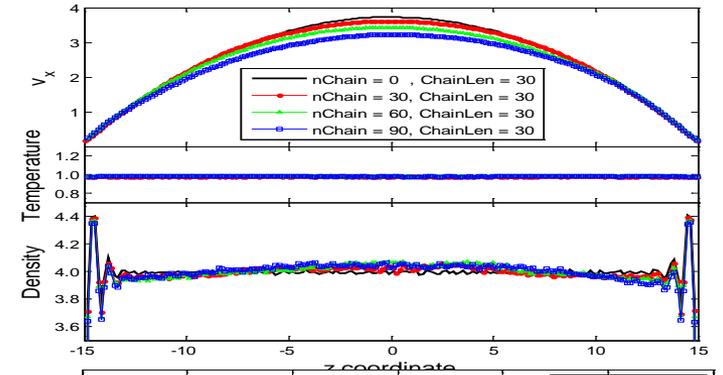
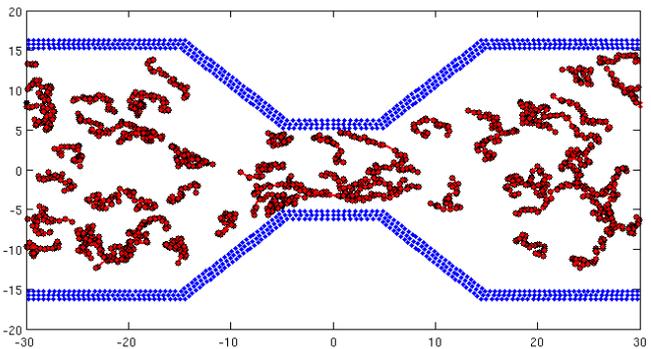
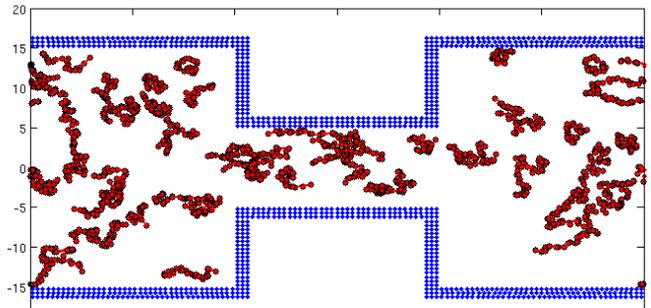
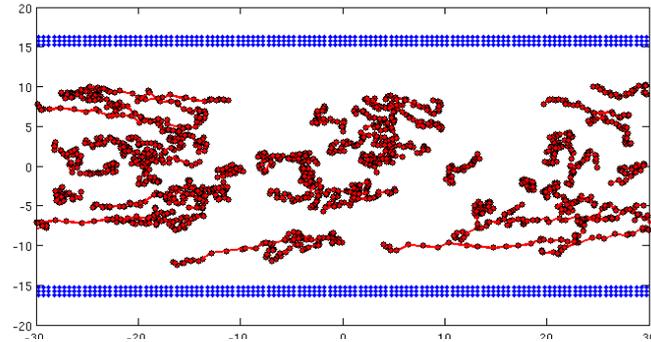
5. Complex fluids in micro channels



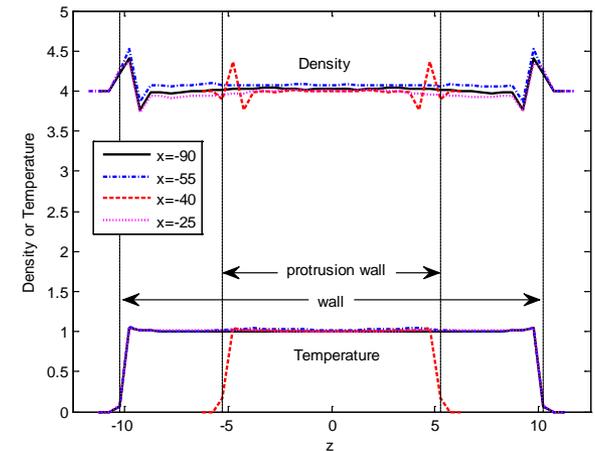
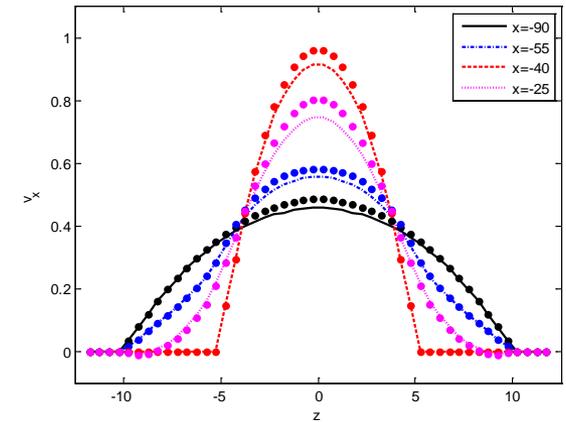
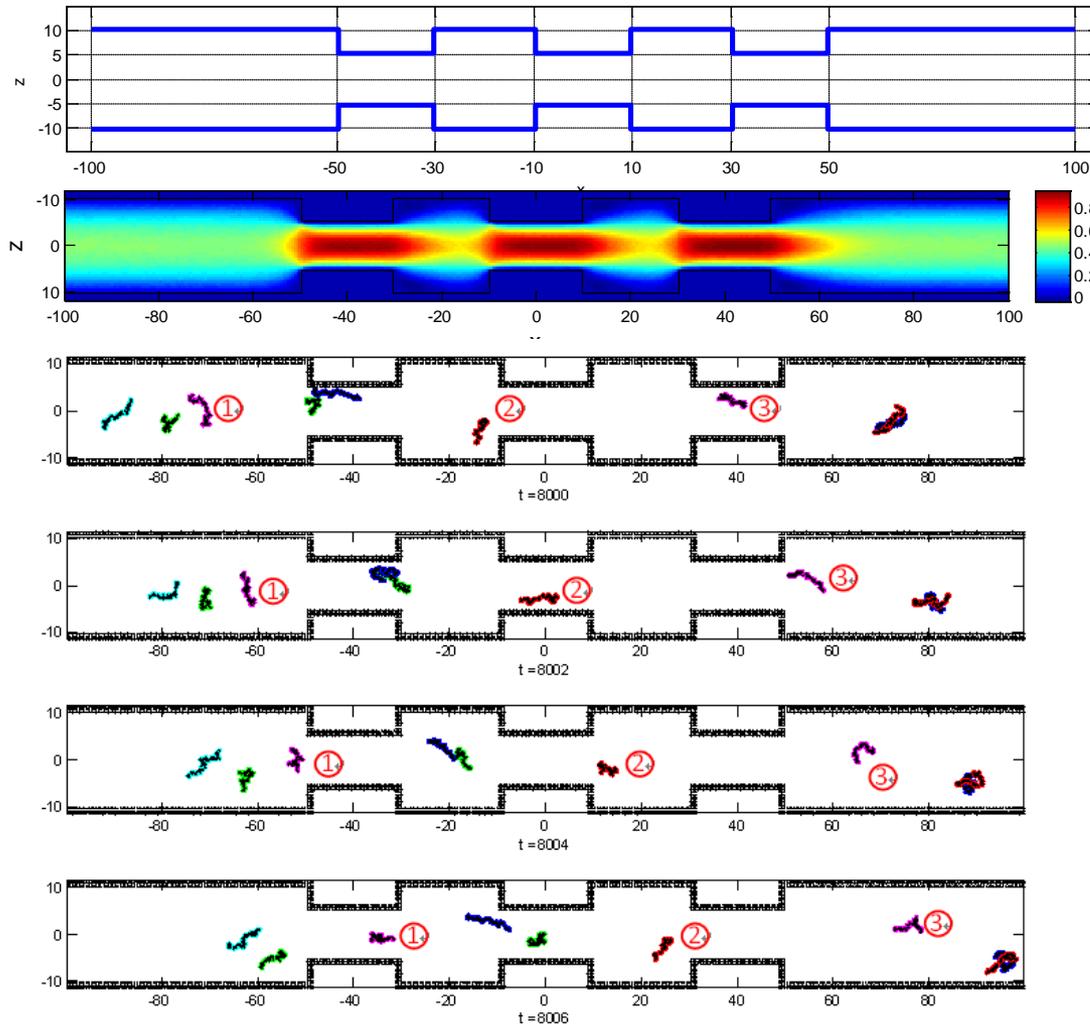
- Micro-devices enable processing, analyzing, and delivering biochemical materials in a wide range of biomedical and biological applications.
- Micro-channels are the main field to deliver and control injected materials. By designing optimal structures of micro-channels or micro-channel networks, it is possible to efficiently control the injection process, either for simple fluids or complex fluids with macromolecules.
- In the device, DNA molecules were observed to undergo **elongation, non-uniform shear and compression**. Near the channel wall, high shear rates results in dramatic **stretching** of the molecules, and may also result in **chain scission** of the macromolecules



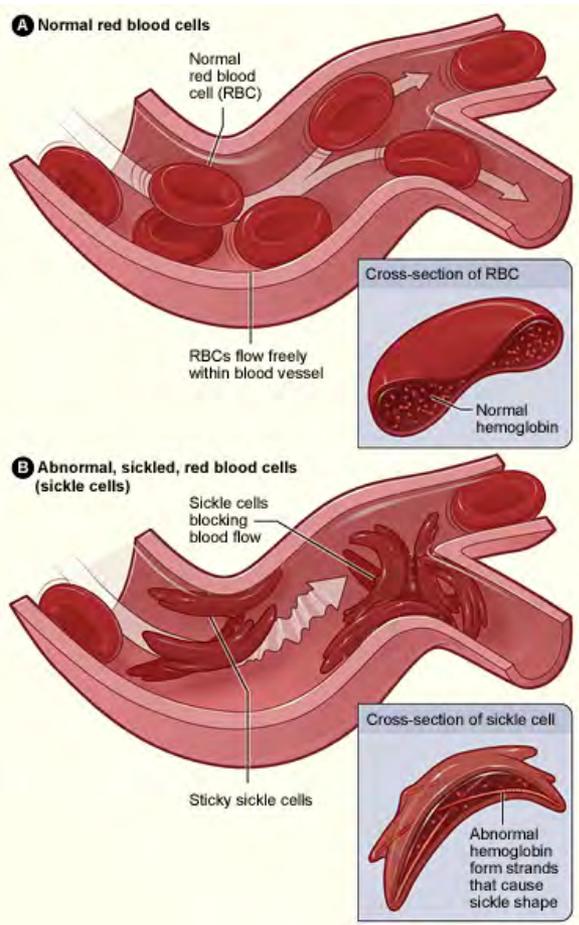
5. Complex fluids in micro channels



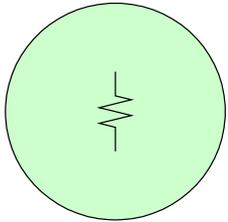
5. Complex fluids in micro channels



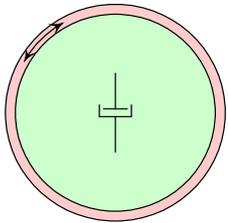
6. Modeling single cells with DPD



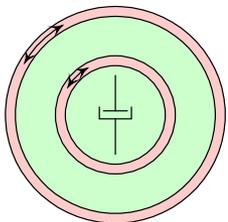
- The study of the movement and deformation of single cells (in blood vessels) is important for understanding mechanical properties of cells.
- The changes in mechanical properties of cells may be closely related to severe cell diseases.
- Modern physiology medicine have established the relationship of mechanical changes between healthy and pathological cells.
- Differences of mechanical properties could be used to distinguish between normal and diseased cells



Solid model



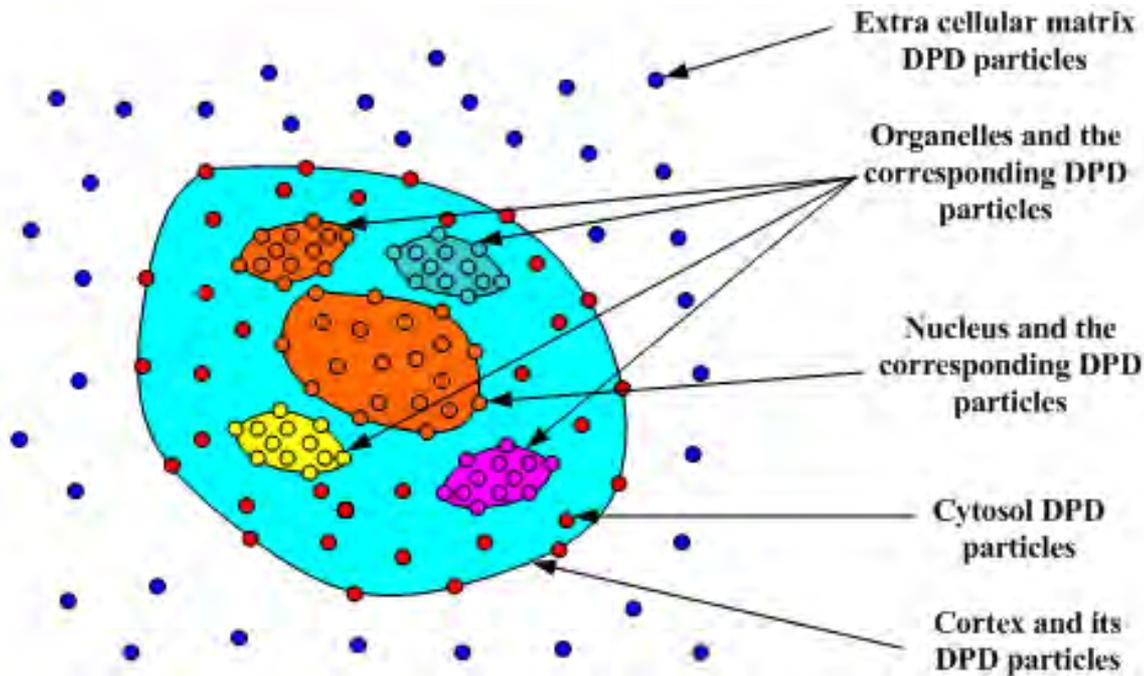
Liquid drop model



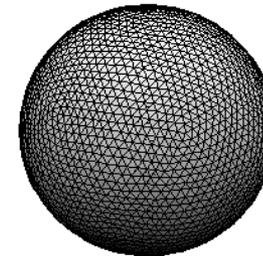
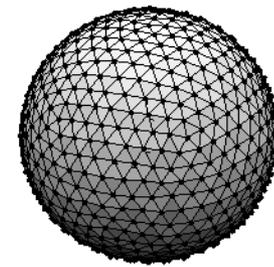
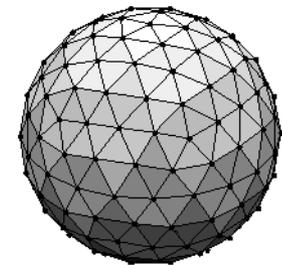
Compound drop model

- **Solid model:** Assuming the whole cell to be homogeneous without considering the distinct cortical layer. For large cell deformations, this model may not work.
- **Liquid drop model:** By treating the cell as a liquid drop, and liquid drop models can be used to model large cell deformation. For cell fast deformations, this model also may not work.
- **Compound drop model:** In order to consider the effects of the nucleus on cell deformation, the compound drop model was developed, which assumes the nucleus to be an encapsulated liquid drop.

6. Modeling single cells with DPD



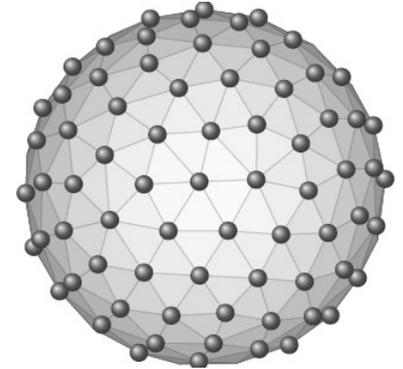
DPD modeling of a cell and its environment



Constructing cell membrane

6. Modeling single cells with DPD

- The cell membrane structure is defined by a 2D triangular network on the spherical surface.
- Each link of triangular network is modeled by nonlinear WLC spring model.
- The force between membrane particles includes the elastic and viscous parts. The elastic part is characterized by an energy potential, given by



$$U(\{\mathbf{r}_i\}) = U_{\text{plane}} + U_{\text{bending}} + U_{\text{area}} + U_{\text{volume}}$$

6. Modeling single cells with DPD

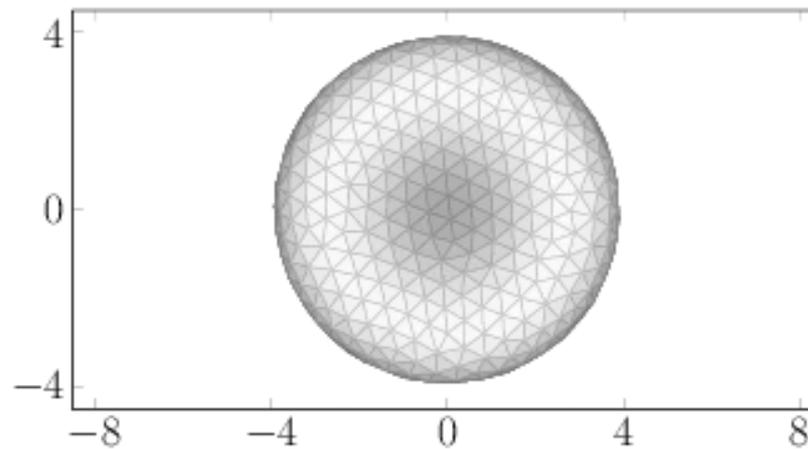
6.1 Biconcave cell (RBC)

- A red blood cell has a biconcave shape. All healthy mammalian RBCs (unstressed shapes) are disc-shaped (discocyte)
- The biconcave discocyte RBC has a flexible membrane with a **high surface-to-volume ratio** that facilitates large reversible elastic deformation of the RBC as it repeatedly passes through small capillaries to deliver oxygen to various parts of the body.
- The pathological RBCs are too stiff to deform sufficiently to traverse narrow capillaries.

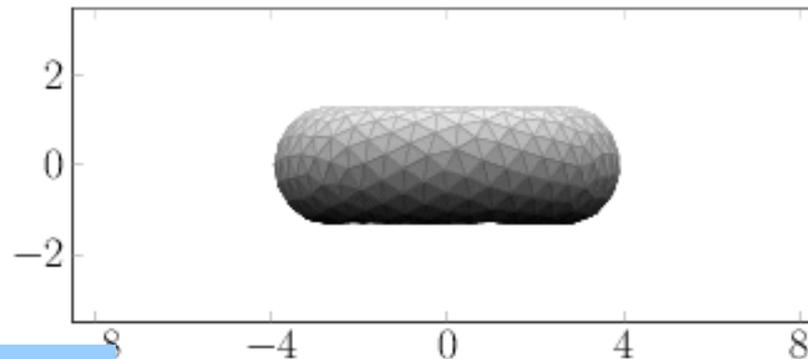
6. Modeling single cells with DPD

6.1 Biconcave cell (RBC)

RBC stretching

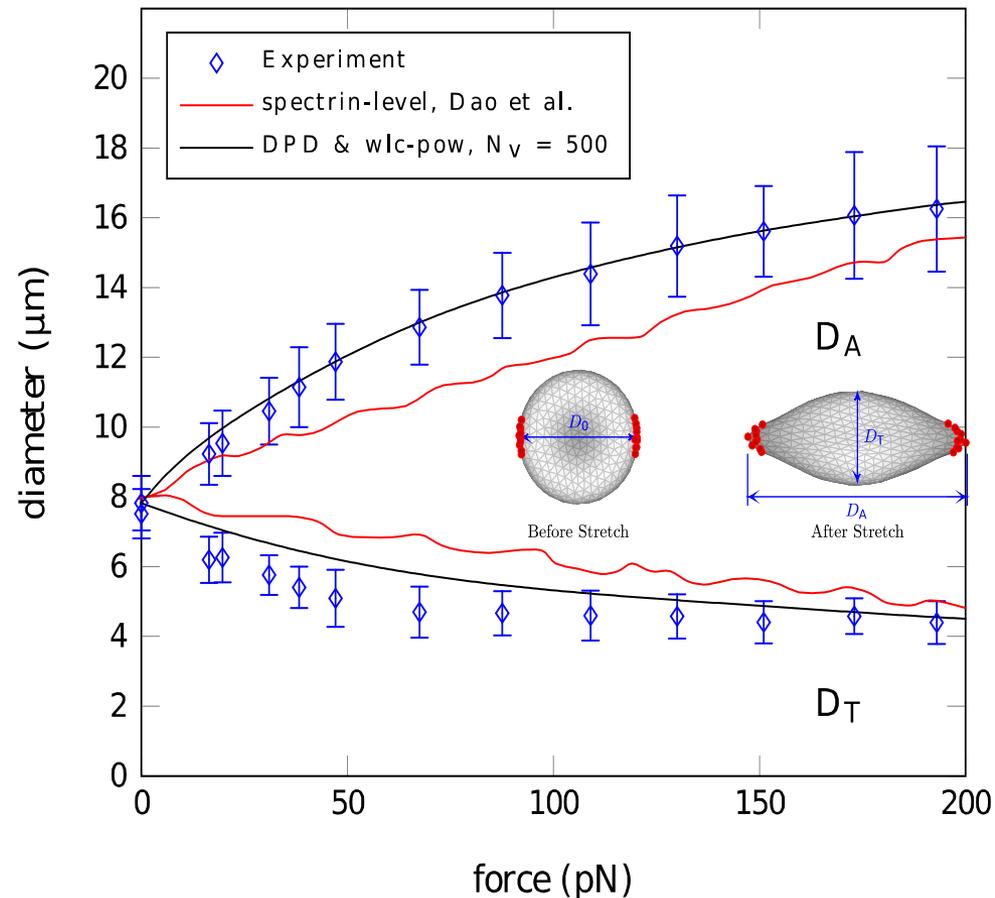
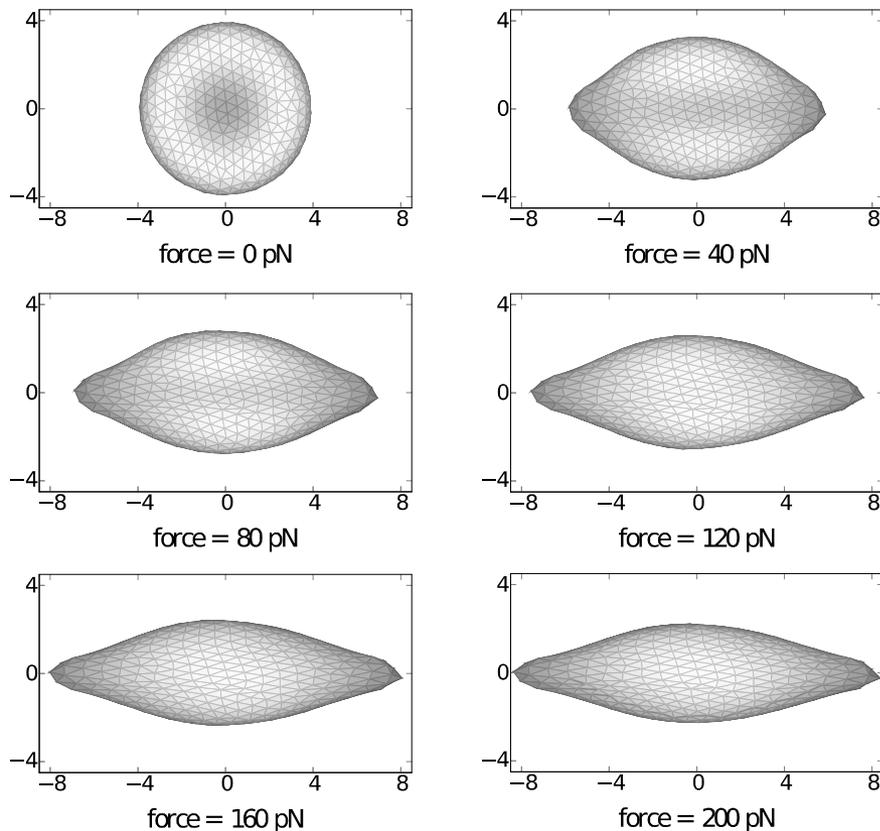


force = 0 pN



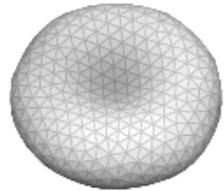
6.1 Biconcave cell (RBC)

RBC stretching



6.1 Biconcave cell (RBC)

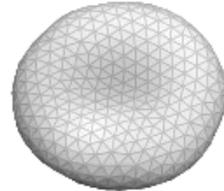
RBCs in shear flows



$$\dot{\gamma} = 10\text{s}^{-1}$$



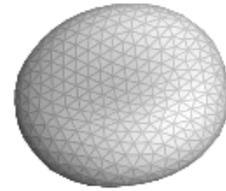
Tumbling



$$\dot{\gamma} = 30\text{s}^{-1}$$



Intermediate



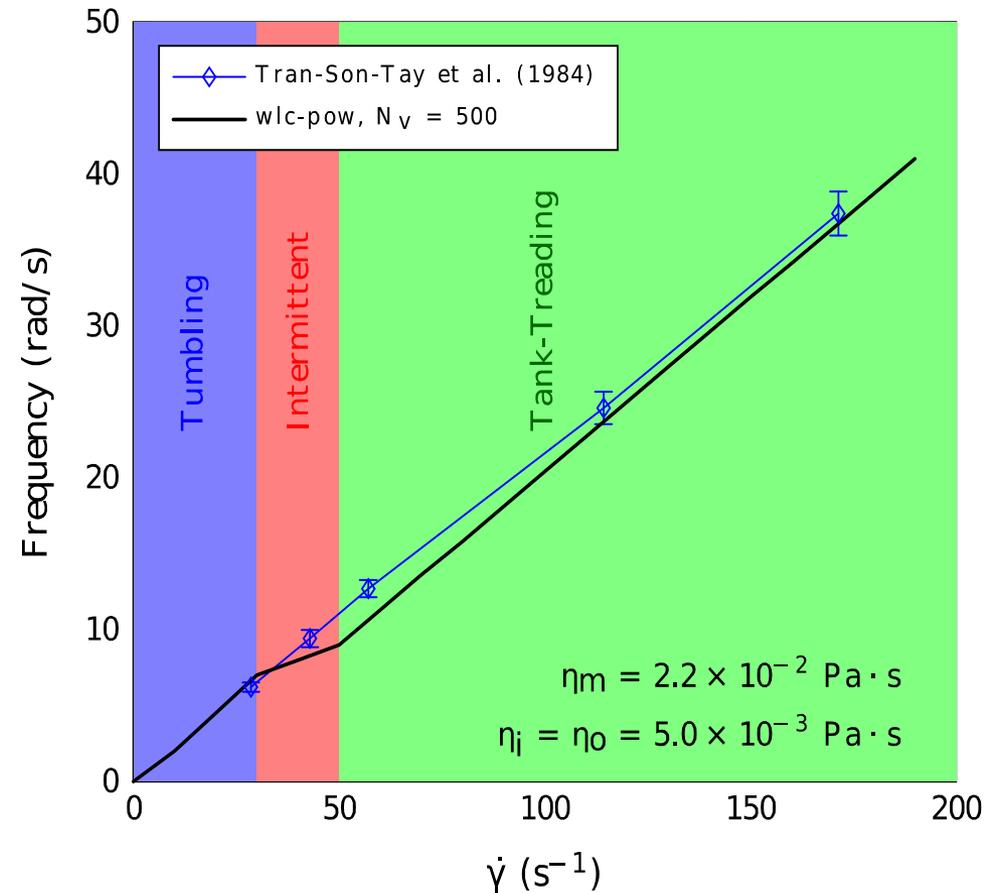
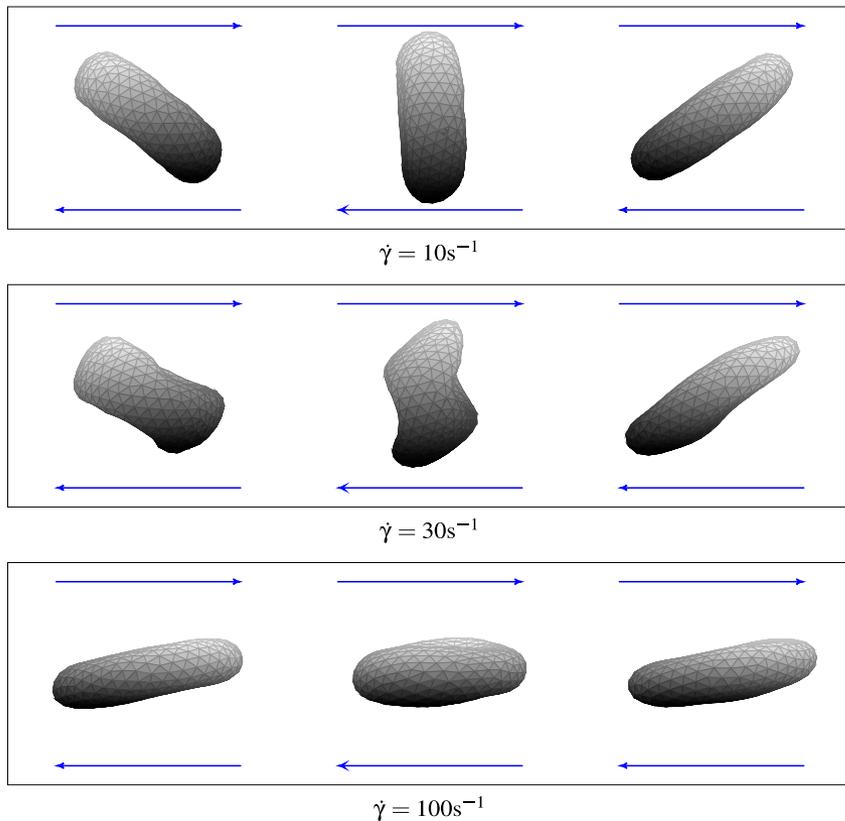
$$\dot{\gamma} = 100\text{s}^{-1}$$



Tank-treading

6.1 Biconcave cell (RBC)

RBCs in shear flows

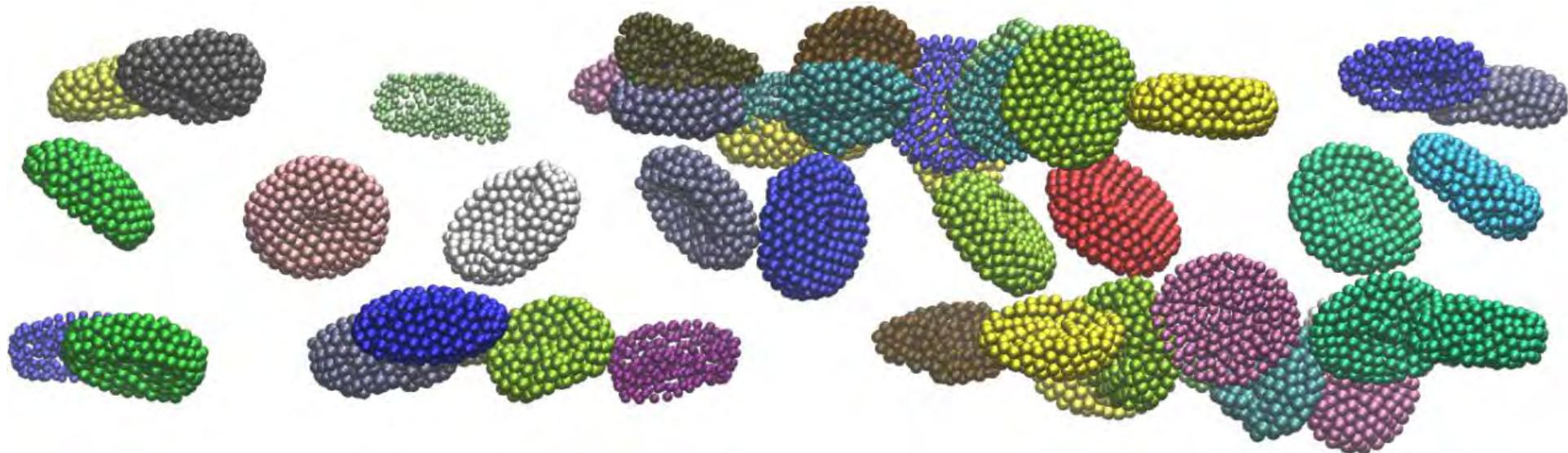


6. Modeling single cells with DPD

6.1 Biconcave cell (RBC)

Multi-RBCs in Poiseuille flow in a tube

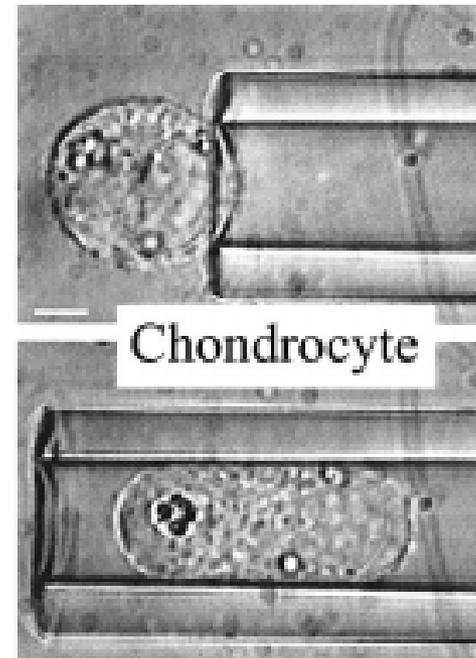
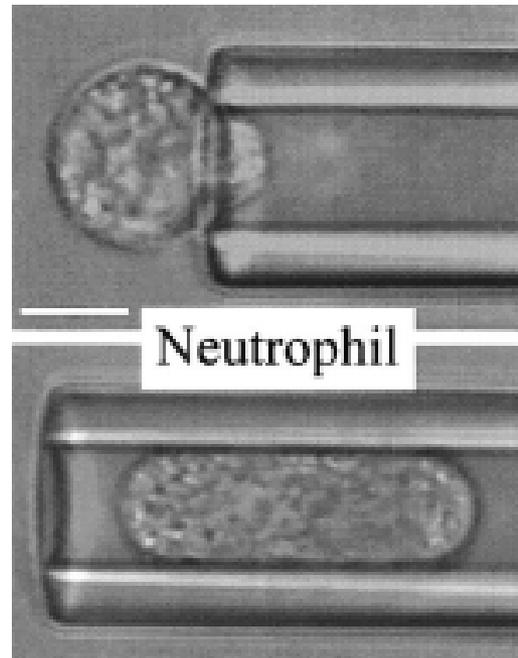
- Based on proper simulations of single RBCs with accurate mechanics, rheology and dynamics, more complicated situations can further be simulated. One of those situations is blood flow.



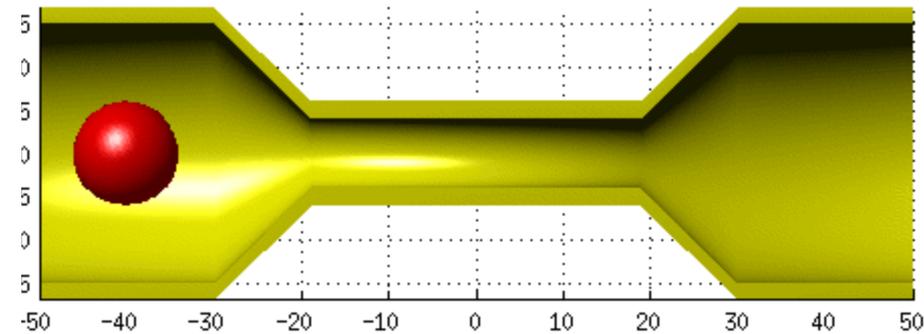
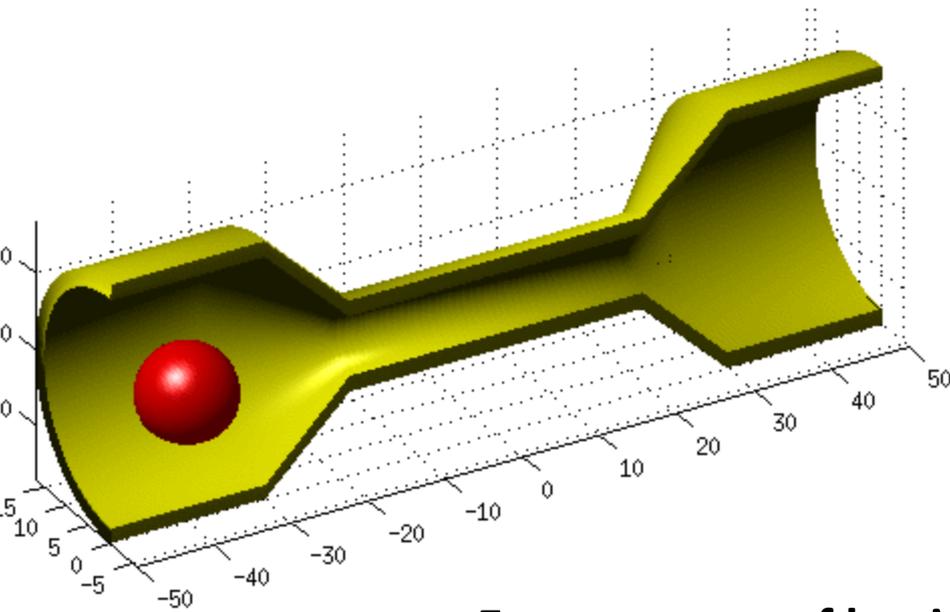
6.2 Spherical cells

Cell passing through channel

The deformation and dynamic response of a cell passing through a micro-channel can be used to investigate the mechanic, physical and biological features of a cell, and thus can be used to cell classification, separation, and disease diagnosis.

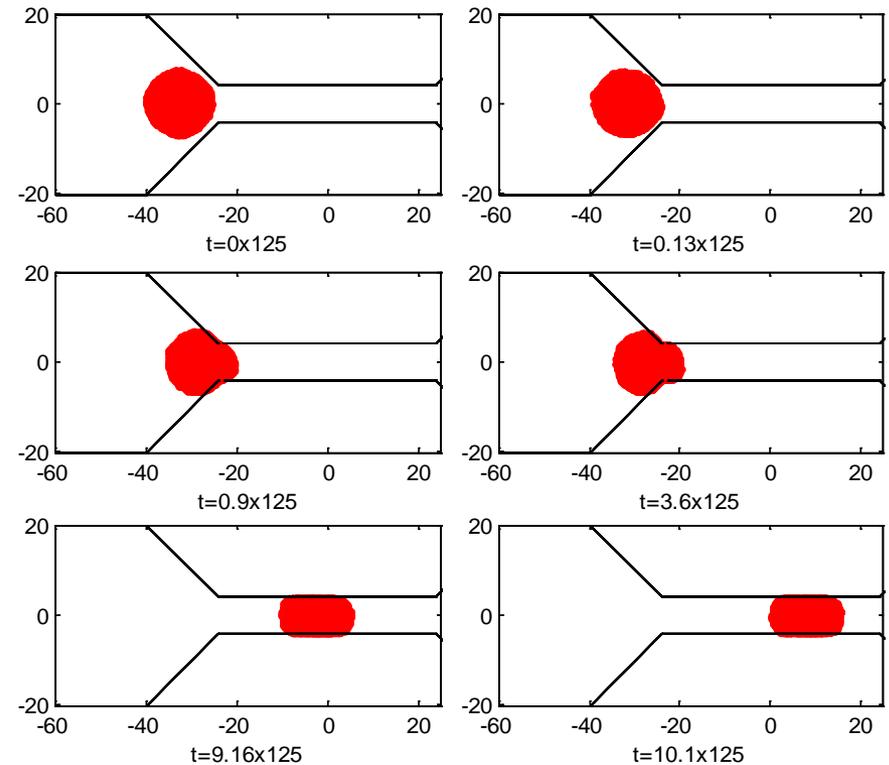
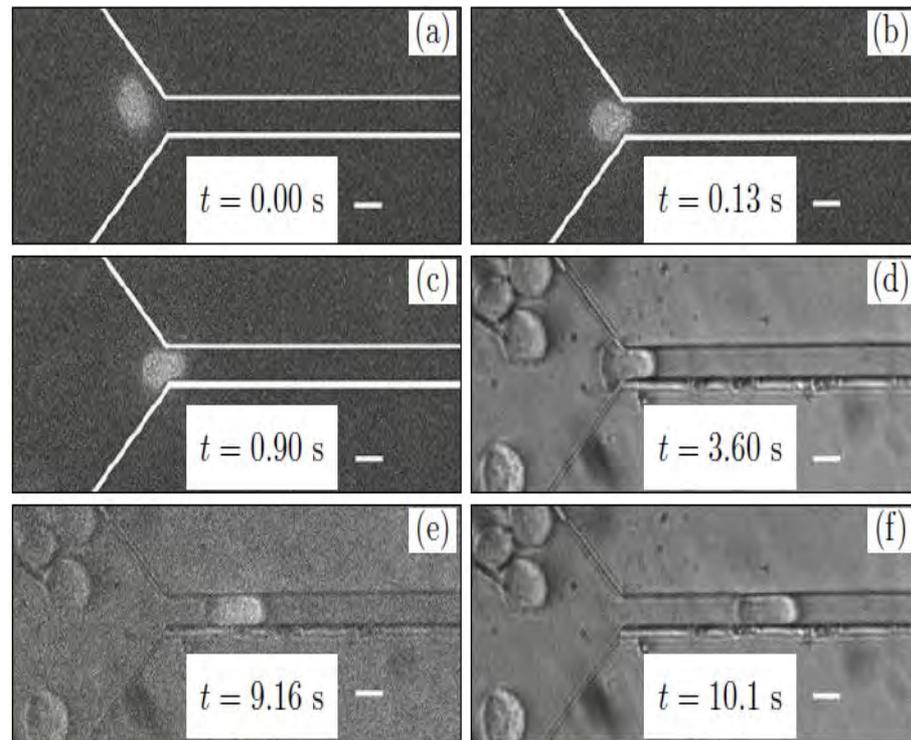


6.2 Spherical cells

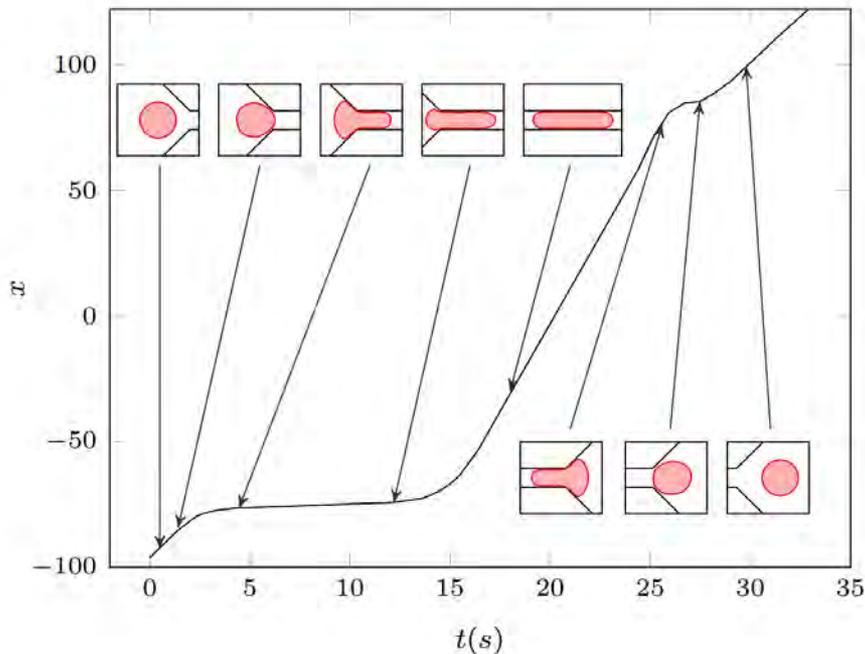


Entry process of benign breast epithelial cells (MCF-10A)

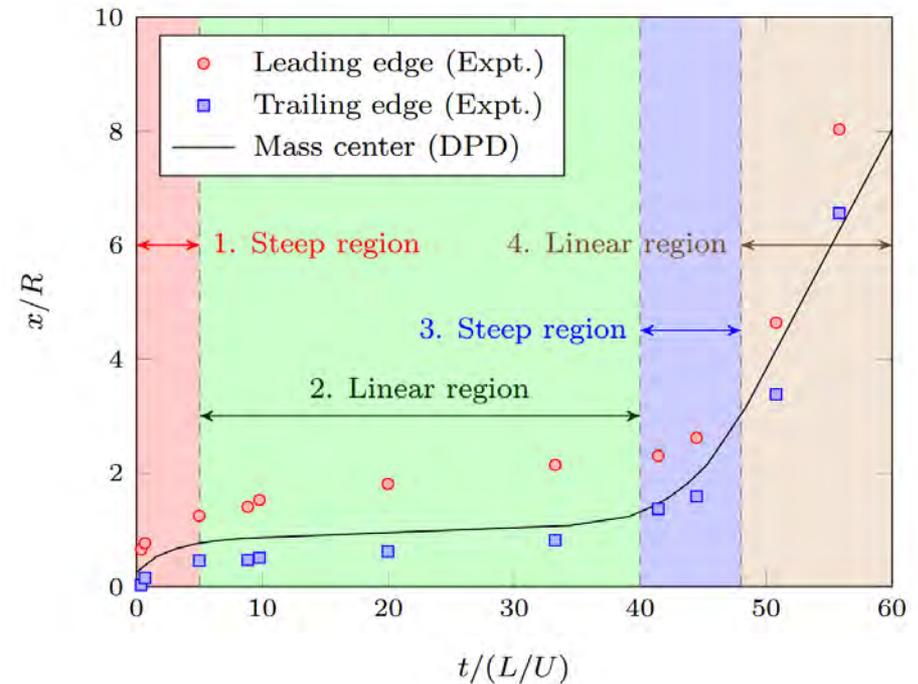
6.2 Spherical cells



6.2 Spherical cells



Cell displacement and deformation pattern



Cell displacement vs experimental data

Approaching (reduce speed) \rightarrow partially enter ($v \rightarrow 0$, long time duration) \rightarrow fully enter (acceleration-roughly constant) \rightarrow partially exit (accelerate suddenly \rightarrow reduce speed)

1. **As a meso-scale particle methods, DPD is attractive and more efficient than classic MD.**
2. **After modification or extension, the DPD method has been applied to different areas including drop dynamics, multiphase flows in complex geometries, and cell modeling.**
3. **DPD need further development:**
 - a. **Interaction potential: for different materials/fluids?**
 - b. **Coarse-graining: to what extent?**
 - c. **Parameter matching: modeling parameter and physical ones?**
 - d. **Multi-scale: possible coupling with or converting to MD or SPH?**
 - e. **Others...**

